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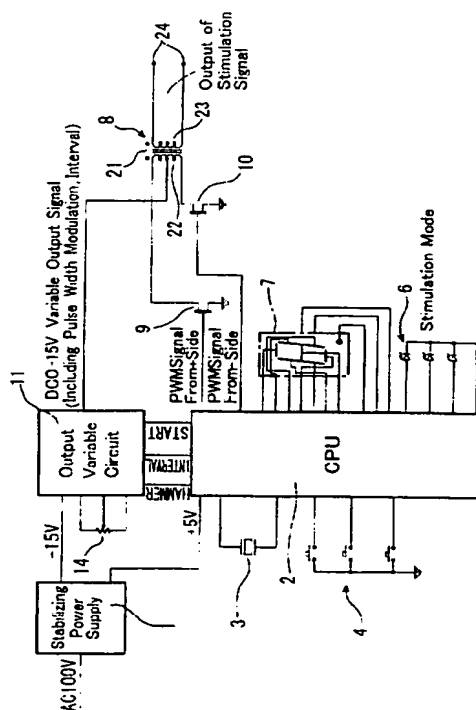
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(54) Living body stimulating apparatus

(57) Living body stimulating apparatus for applying an electric stimulus to a living body, said apparatus comprising electrodes to apply a stimulation signal to said living body and a stimulation signal generator (8,9,10),

said stimulation signal generator being adapted to generate a stimulation signal from a periodic signal of predetermined recurrence frequency ($1/T$), said stimulation signal comprising groups (S) of pulse width modulated pulses, recurring at said predetermined frequency.

FIG. 1



Description

[0001] The present invention relates to a living body stimulating apparatus, such as a low-frequency electrotherapeutic device. More particularly, the present invention concerns a stimulating apparatus of the kind comprising a conductor element with a built-in electrode which can be attached to a living body. Stimulation is achieved by an electric current flowing through the electrode into the living body.

[0002] In general, such a living body stimulating apparatus is used for the treatment of a nerve function in a diseased part, by allowing a low frequency pulse current to flow in the diseased part, said low frequency pulse current being output from a transmitter to an electrode. In Japanese Patent Un-Examined Publication No. 1-146562, for example, is disclosed a living body stimulating apparatus which enables the control of the speed and intensity of stimulation, by switching stimulation signals output from an output circuit to a living body (or human body). The stimulation signals are either DC intermittent pulses for periodically outputting positive pulses, AC intermittent pulses for periodically outputting rectangular wave pulse groups consisting of positive pulses and negative pulses, alternate intermittent pulses for periodically and alternately outputting positive pulses and negative pulses, the period or amplitude of which can be varied.

[0003] However, it is generally difficult to make pass a DC current through a human body, since it has a resistance of about 100k Ω , depending upon voltage, whilst a highfrequency AC current flows easily through a human body. For example, a human body exhibits a resistance of about 1k Ω under an AC voltage of 1kHz, said resistance being reduced by half if the frequency doubles. In other words, a human body has a capacitive impedance, and thus the in-vivo resistance tends to decrease as frequency increases. On the other hand, as the stimulation of the human body is concerned, low frequencies close to direct current, and rectangular waves comprising a high DC component are more stimulative. Thus, for the same frequency, sinusoidal waves will induce softer stimuli than rectangular waves.

[0004] Fig.5 illustrates an example of a conventional living body stimulating apparatus for applying stimulation signals having the form of sine waves to a human body. As shown, numeral 101 designates a CPU (central processing unit) as controlling means. The CPU outputs digital data signals which are converted into analogue data signals by the D/A converter 102. Then, the analogue data signals are amplified by an amplifier 103, to provide sine-wave stimulation signals between conductive elements or output electrodes 105, over a transformer 104. The amplitude of the sine wave can be increased or decreased by operating a variable gain element 106 at the input of the amplifier 103.

[0005] Although a sinusoidal wave induces a soft stimulation of the human body, it comprises only one frequency component, which leads to a very limited therapeutic effect. Furthermore, the output circuit of such a conventional apparatus requires analogue circuits such as the D/A converter 102 and the amplifier circuit 103

which are necessary for obtaining a substantially sinusoidal waveform. The number of components is relatively high and the structure of the circuit is complex, thus leading to low power efficiency. In other words, conventional circuits outputting sinusoidal waves would require dozens of components such as transistors, resistors and capacitors.

[0006] It is a main object of the invention to solve the problems recited above and to propose a living body stimulating apparatus which provides extensive therapeutic effects while soft stimuli are applied to the living body.

[0007] To attain the above objects, there is proposed a living body stimulating apparatus as defined in the appended claims

[0008] Other objects, features and advantages of the invention will be apparent to those skilled in the art from the following description of the various embodiments of the invention, wherein reference is made to the accompanying drawings, of which:

Fig.1 is a circuit diagram showing a living body stimulating apparatus in accordance with a first embodiment of the invention;

Fig.2 is a waveform diagram showing waveforms at several points in the apparatus of Fig. 1;

Fig.3 is a waveform diagram of a stimulating signal when a dummy resistance is connected between the output electrodes of the apparatus;

Fig.4 is another waveform diagram of a stimulating signal when the output electrodes of the apparatus are applied onto a human waist;

Fig.5 is a circuit diagram showing a conventional living body stimulating apparatus.

[0009] First, an overall structure of an apparatus of the invention will be described with reference to Fig.1. Reference numeral 1 designates a stabilized power supply unit connected to an AC source and providing a DC stable voltage. In the embodiment, AC source voltage of AC 100 V is converted into DC voltages of DC+15V and DC+5V, respectively. Reference numeral 2 designates a CPU (central processing unit) which serves as a control means powered by said DC+5V from the said stabilized power supply unit 1. The CPU inputs reference clock signals from a crystal oscillator 3. As well known in the art, CPU 2 is integrated with an input/output means, a processing means, a memory means in which a control sequence is stored, said control sequence being able to generate predetermined patterns of stimulating electric signals.

[0010] To an input port of said CPU 2 are connected a plurality of switches 4 for selecting a specific stimulation mode from among several stimulation modes. A plu-

ality of LEDs 6 are connected to an output port of said CPU 2 for displaying which stimulation mode is currently active. Furthermore, to the output port of the CPU 2 are connected a segment LED 7 as time display means for counting and displaying the stimulation time, two FETs 9, 10 included in the stimulus signal generating means 8, and an output-variable circuit 11 for varying the amplitude and interval (pause) of stimulating signals to be applied to a living body. For the sake of simplicity, only one segment LED 7 is illustrated in the present embodiment, but two or more segment LEDs 7 could be connected in parallel. Alternatively, the foregoing LEDs 6 and the segment LED 7 may be integrated together in a common LCD display.

[0011] The output-variable circuit 11 is powered by the DC voltage of DC+15V provided by the stabilized power supply unit 1 and receives control signals from the CPU 2, namely the strong stimulation control signal (HAMMER), the stimulation pause setting signal (INTERVAL), and the stimulation start signal (START). The circuit 11 outputs a variable output signal. A manually operable variable resistor 14 is provided for setting the level of the variable output signal. The variable output signal is supplied to the stimulus generator means 8. This signal has a rectangular waveform of predetermined recurrence frequency and its amplitude is modulated in the range DC 0V to DC+15V.

[0012] The stimulus generator means 8 subjects the variable output signal from the output-variable circuit 11 to pulse width modulation. The stimulus generator comprises FETs 9, 10 serving as switching means and a transformer 21, the primary and secondary sides of which are insulated from each other. More specifically, the primary winding 22 of the transformer 21 has a center tap connected to the variable output signal line of the said output-variable circuit 11, while the secondary winding 23 have ends connected to a pair of output electrodes 24 serving as conductive elements. The drain of the grounded source FET 9 is connected to one end of the primary winding 22 of the transformer 21, while the drain of the other source grounded FET 10 is connected to the other end of the primary winding 22. The + side PWM signals from the CPU 2 are supplied to the gate of the FET 9, while - side PWM signals from the CPU 2 are supplied to a gate of the FET 10.

[0013] Next, the action of the above-structured apparatus will be explained with reference to the waveform diagram of Fig.2, in which the uppermost waveform shows a variable output signal from the output-variable circuit 11, followed by the respective waveforms of the + side PWM signals, - side PWM signals and the stimulation signals between the output electrodes 24.

[0014] If a specific stimulation mode is selected by the switch 4, and then a start switch (not shown) is operated, the LED 6 corresponding to the specific stimulation mode selected is switched on by the CPU 2. The CPU 2 controls also the stimulus generator means 8 and the output-variable circuit 11 in order that the stimulation

signals corresponding to the selected stimulation mode are output between the electrodes 24. The stimulation start signal is supplied from the CPU 2 to the output-variable circuit 11, and the variable-output signal is supplied from the output-variable circuit 11 to the stimulus generator means 8. As shown in Fig. 2, the variable-output signal comprises rectangular pulses defined by an amplitude A1 and a time width t1, repeating at a period T. The amplitude A1 can be varied by operating the variable resistor 14 in the range DC0V to DC+15V and thus it is possible for a user to change the degree of stimulation to a desired level. Alternatively, the period T and time width t1 can be varied by the CPU 2 (not shown in the drawing). In such an embodiment a user may obtain a more desirable stimulus by varying a parameter of the control program inside the CPU 2.

[0015] Every time a rectangular wave pulse is output from said output-variable circuit 11, the CPU 2 is enabled to output on-pulses to the FET 9 or the FET 10, during the output period of the rectangular pulse. The on-pulses have a higher frequency component than the rectangular pulse. The time width t2 of each on-pulse to the FET 9 or FET 10 gradually increases from the rising edge of said rectangular pulse until about the middle of said rectangular wave pulse and then gradually decreases until the falling edge of said rectangular pulse.

[0016] When the +side PWM signal is supplied from the CPU 2 to the FET 9 while a rectangular pulse is output to the center tap of the primary winding 22 of the transformer 21, the FET 9 is turned on during each on-pulse, so that the primary side (i.e. dotted side) of the primary winding 22 is grounded, thus inducing a voltage in the primary side (dotted side) of the secondary winding 23. Likewise, when the -side PWM signal is supplied from the CPU 2 to the FET 10 while a rectangular wave pulse is output to the center tap of the primary winding 22 of the transformer 21, the FET 10 is turned on during the output period of the on-pulse, so that the secondary side (i.e., non-dotted side) of the primary winding 22 is grounded and thus inducing a voltage in the secondary side (non-dotted side) of the secondary winding 23. Accordingly, as shown in Fig.2, the supply of the on-pulses to the gate of the FET 9 during the output period of the rectangular wave pulses allows a positive stimulation signal to be output, while the supply of the on-pulses to the gate of FET 10 during the output period of a rectangular wave pulse allows a negative stimulation signal to be output.

[0017] Thus, between the output electrodes 24 are repeatedly generated stimulation signals having a voltage level proportional to the amplitude A1, said signals being obtained by subjecting the rectangular wave pulses of the variable-output signals to pulse width modulation (PWM) through the FETs 9, 10. These stimulation signals exhibits a group S of pulses, generated at every period T, the group having the time width t1, said pulse group S alternately having a positive voltage and a negative voltage. The time width t2 of each on-pulse grad-

ually increases from the beginning of the pulse group until the middle thereof and then gradually decreases until the group S ends. As long as a stimulation signal is output, a built-in timer (not shown) inside the CPU 2 is allowed to count time, and displays the time on the segment LED 7.

[0018] Fig.4 shows a waveform diagram of a stimulation signal which is actually applied to a human body. The stimulation signal shown here is defined by a rectangular wave pulse of recurring frequency 2.8kHz ($T=357\mu\text{Sec}$). High frequency components are provided by varying the time width t_2 in the range 10 to 60 μSec . Fig. 3 shows a comparative waveform in the case a 500 Ω dummy resistor is connected as a load between the output electrodes 24. In that case, substantially the same waveform as that of the stimulation signal of Fig. 2 is generated between the terminals of the dummy resistor. In contrast, Fig.4 shows a waveform in a case where the output electrodes 24 are attached to a human waist and then energized. In that case, the human body functions as if it were a capacitive element and the waveform of the rectangular wave pulse group S is distorted into a low frequency sinusoidal wave. Accordingly, an extremely soft feeling of stimulation is obtained as compared with rectangular waves of the same frequency and current. Furthermore, since the stimulation signals comprise high frequency components (obtained by switching the FETs 9 and 10) the therapeutic effects are enhanced.

[0019] In order that the stimulation signals exhibit a sinusoidal waveform such as the one illustrated in Fig. 4, when applied to a human body, it is desirable that the rectangular pulses defining pulse groups S are alternately positive and negative, at intervals of period T. Furthermore, the time width t_2 of a PWM pulse (on-pulse) is gradually increased during the first half of the pulse group S and then gradually decreased during the second half thereof. It should be noted that the on-pulse time width t_2 can be varied by a time width varying means or a control sequence of the CPU 2. In addition, various waves such as triangular waves or pre-distorted waves can also be envisaged, thus enabling a unique stimulation feeling different from the one provided by sinusoidal waves.

[0020] When the above-mentioned stimulation signals are repeatedly applied to a human body, the latter may get accustomed to these signals and the therapeutic effects such as the removal or alleviation of pains are consequently lowered. In a further embodiment of the invention, the control sequence of the CPU 2 comprises pauses. The stimulation signal is temporarily stopped during the output of a stimulation pause setting signal from the CPU 2 to the output variable circuit 11. The stimulation pause setting signal indicates a stimulation pause period. Another way to prevent inurement to stimulation is to vary the amplitude of the stimulation signal. In response to the strong stimulation command signal output from the CPU 2, a rectangular pulse of larger am-

plitude A2 than the predetermined amplitude A1 is temporarily supplied by the output variable circuit 11 to the stimulus generator means 8. Thus, stronger stimulation signals i.e. pulse groups S' of greater amplitude are temporarily applied to the living body and the above-mentioned drawback is eliminated.

[0021] Since the stimulus generator means 8 modulates the pulse width of on-pulses within a rectangular pulse recurring at a given frequency, the resulting signal applied to the living body comprises components of higher frequency than said recurrence frequency. The human body having a capacitive impedance as mentioned above, the higher the frequency of a component of the signal, the lower the impedance at this frequency. It follows that the waveforms of the rectangular pulse groups are distorted as a whole, thereby generating softer feeling of stimulation as compared with the rectangular wave pulses of the same current and frequency. In addition, as each rectangular pulse group S includes signal components of higher frequency than the recurrence frequency of the rectangular wave pulse, extensive therapeutic effects can be obtained.

[0022] Moreover, the stimulus generator means 8 of the invention comprises the FETs 9 and 10 serving as switching means for on-off switching the rectangular wave pulse to thereby produce the rectangular wave pulse group S which includes signal components having higher frequency than the recurrence frequency. The CPU 2 serves as pulse width control means for supplying the FETs 9 and 10 with PWM digital signals (or +side PWM signals and -side PWM signals) for switching the FETs 9, 10.

[0023] To distort each rectangular wave pulse of the stimulation signal, the FETs 9, 10 (serving as switch means) are controlled with on-off PWM digital signals. There is therefore no need for conventional analogue circuit (such as the conventional D/A circuit 102 and the amplifier circuit 103) for obtaining the sinusoidal waveform. As a result, whilst conventional circuit for outputting sinusoidal waves would require dozens of components such as transistors, resistors and capacitors, the apparatus according to the present embodiment of the invention only requires a pair of FETs 9, 10, thus extremely simplifying the structure of the stimulus generator means 8 serving as the stimulation signal output circuit. Further, the pulse width modulation using the switch means exhibits very high power efficiency, as known in the domain of motor inverters.

[0024] The CPU 2 of the embodiment of the invention comprises strong stimulation controlling means for controlling the rectangular wave pulse amplitude: when strong stimulation mode is active, the rectangular wave pulse amplitude has an amplitude A2 which is greater than the predetermined amplitude A1. The strong stimulation controlling means enables therefore to apply stronger stimulation signals i.e. rectangular wave pulse groups S' of larger amplitude. This prevents a human body to get accustomed to the stimulation signals. Fur-

thermore, the apparatus can be adapted to generate a rectangular wave pulse whose amplitude is randomly variable. Similarly, the pause period of the stimulation signal can also be made random. In both cases, a human body is more effectively prevented from getting accustomed to the stimulation signals. In addition, since the control sequence running on the CPU carries out the respective functions of said strong signal command means, stimulation pause command means as well as pulse width control means, the circuit has a less complicated structure than those known from the prior art.

[0025] The recurrence frequency of the rectangular wave pulse groups, the time width t_1 of the rectangular wave pulse group S, the number and width t_2 of the individual PWM pulses (on-pulses) may be chosen relatively freely according the various needs.

Claims

1. Living body stimulating apparatus for applying an electric stimulus to a living body, said apparatus comprising electrodes to apply a stimulation signal to said living body and a stimulation signal generator (8.9.10), said stimulation signal generator being adapted to generate a stimulation signal from a periodic signal of predetermined recurrence frequency ($1/T$), **characterised by** said stimulation signal comprising groups (S) of pulse width modulated pulses, recurring at said predetermined frequency.
2. Living body stimulating apparatus according to claim 1, **characterised in that** said periodic signal is a rectangular wave pulse signal consisting of rectangular pulses of predetermined width (t_1) recurring at said predetermined recurrence frequency and that the stimulation signal generator is adapted to generate groups of PWM pulses, having said predetermined time width (t_1) and sequentially alternating signs, the time width (t_2) of a PWM pulse of a group (S) gradually increasing during the first half of said group (S) and gradually decreasing during the second half thereof.
3. Living body stimulating apparatus according to claim 2, **characterised in that** said stimulus generator comprises switching elements (9,10) for on-off switching said rectangular wave pulse signal, said apparatus further comprising pulse width control element (2) for switching the switching elements (9,10) with PWM digital signals
4. A living body stimulating apparatus according to claim 3, **characterised in that** said PWM digital signals are produced by a control sequence of a CPU (2).
5. A living body stimulating apparatus according to

claim 2, **characterised in that** it comprises a strong stimulation controlling element generating a strong stimulation controlling signal (HAMMER) for temporarily outputting said rectangular wave pulse signal at a larger amplitude than at a predetermined one.

6. A living body stimulating apparatus according to claim 5, **characterised in that** said strong stimulation controlling signal is generated by a control sequence of the CPU (2).
7. A living body stimulating apparatus according to claim 1, **characterised in that** it comprises a signal pause setting element generating a signal pause setting signal (INTERVAL) for temporarily stopping the output of said stimulation signal.
8. A living body stimulating apparatus according to claim 7, **characterised in that** said the pause period of the stimulation signal is randomly varied.
9. A living body stimulating apparatus according to claim 7 or 8, **characterised in that** said stimulation pause setting signal is generated by a control sequence of a CPU (2).
10. A living body stimulating apparatus according to claim 2, **characterised in that** the amplitude of said rectangular wave pulse is randomly varied.

FIG. 1

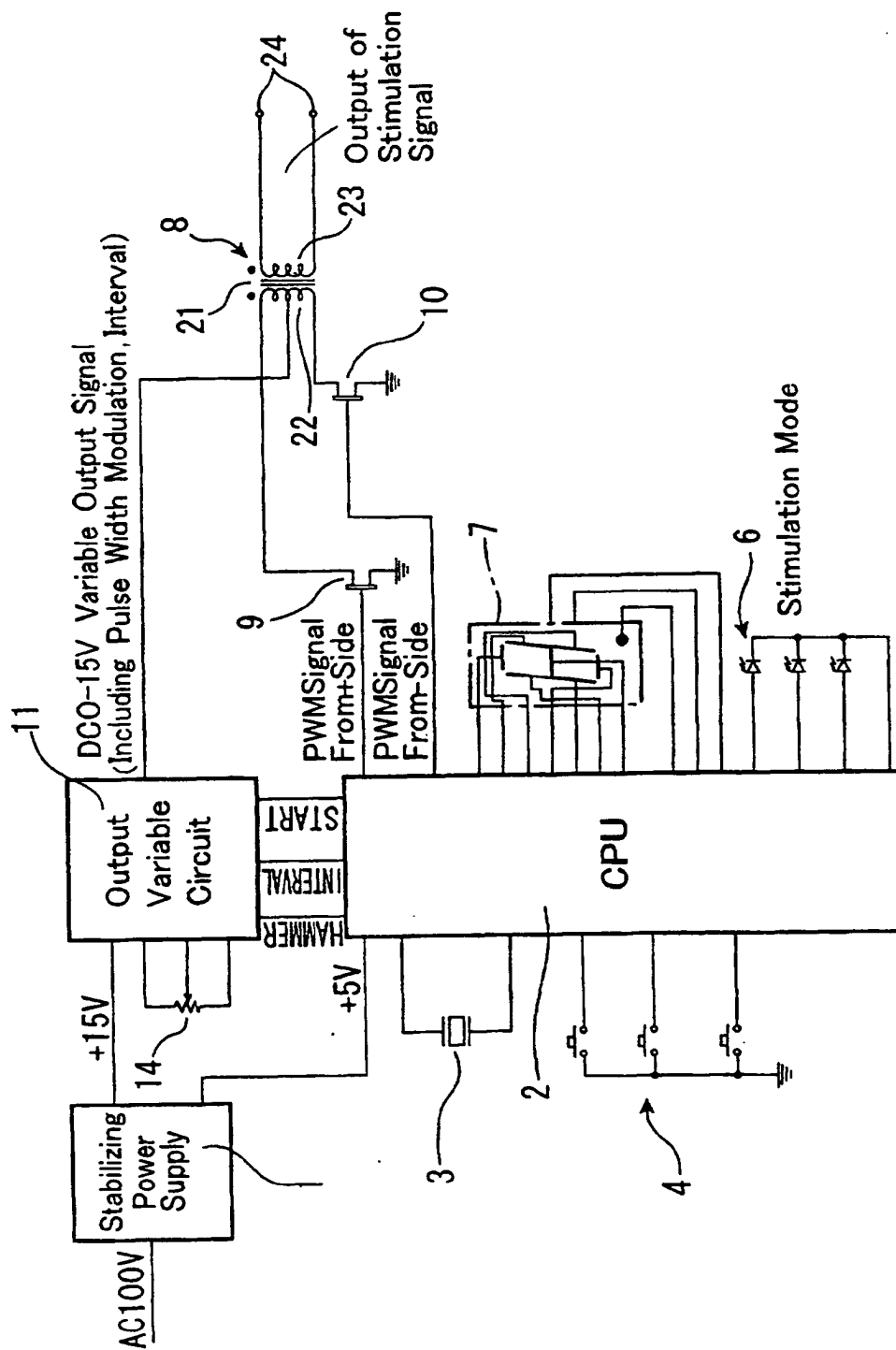


FIG. 2

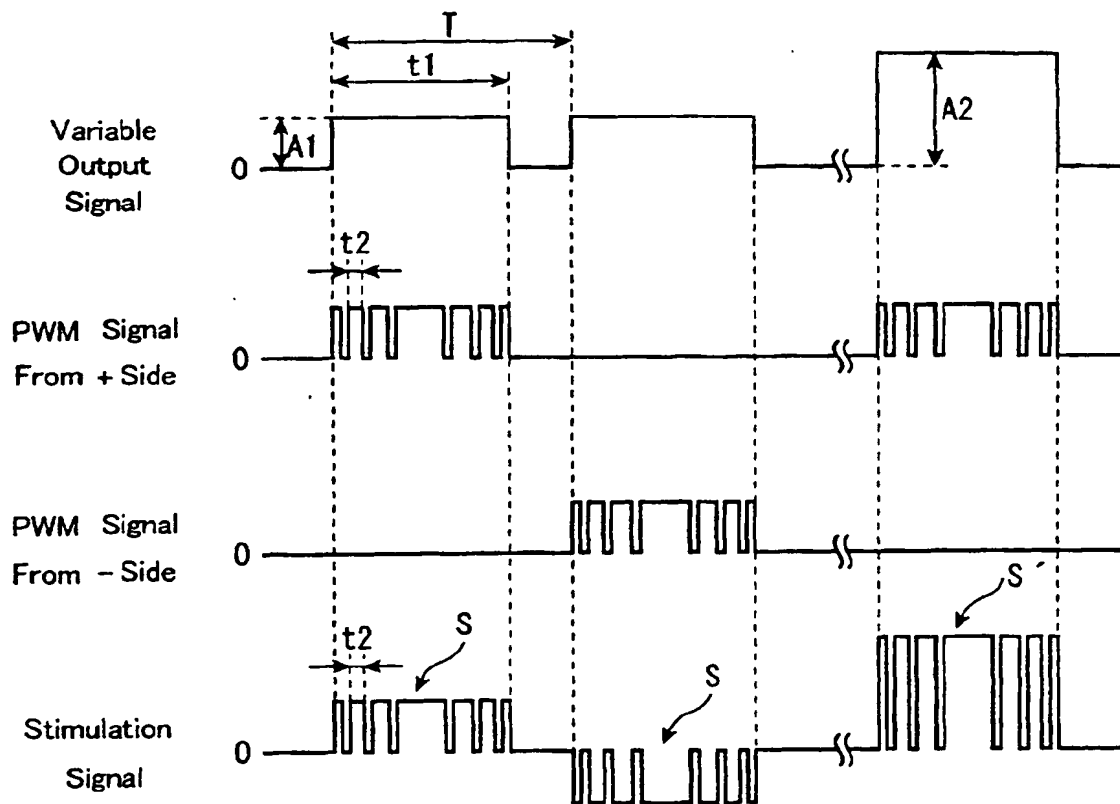


FIG. 3

Waveform in a case a where the apparatus is connected to 500 Ω load,

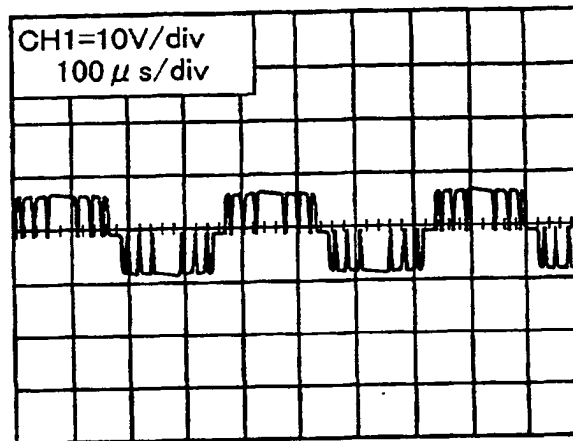


FIG. 4

Waveform in a case a where the apparatus is connected to a human waist

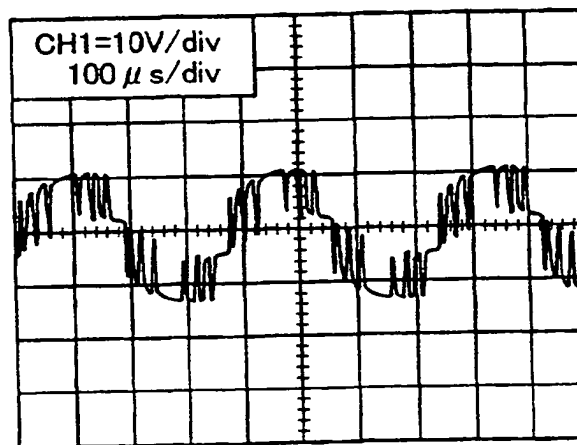
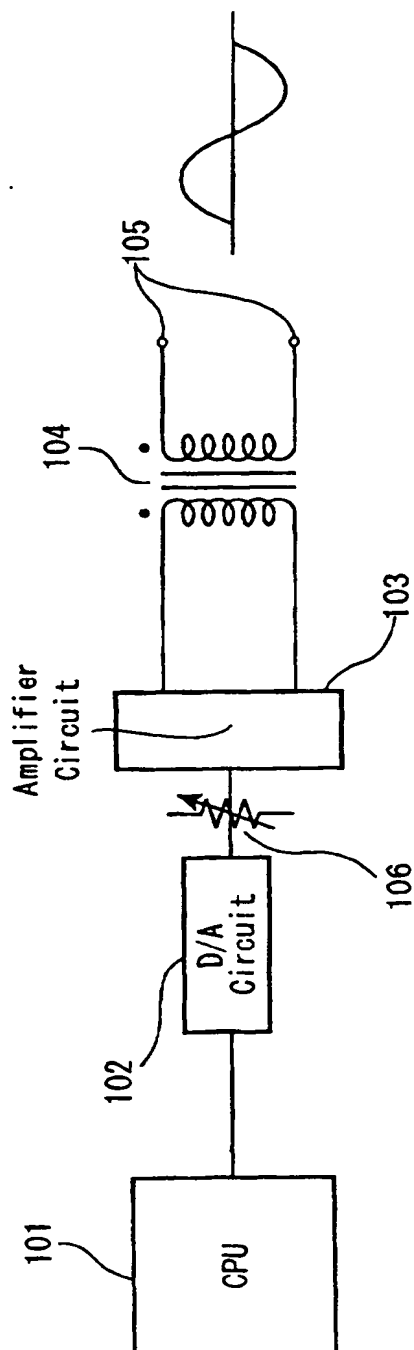


FIG. 5





European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 01 40 0186

DOCUMENTS CONSIDERED TO BE RELEVANT				
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)	
X	US 4 938 223 A (CHARTERS THOMAS H ET AL) 3 July 1990 (1990-07-03) * column 2, line 5 - column 4, line 53 *	1,7,9	A61N1/36	
Y	* claims 1-11,18; figures *	2-6,8,10		
X	US 5 836 081 A (OROSZ JR STEVEN J) 17 November 1998 (1998-11-17)	1,7,9		
Y	* the whole document *	2-6		
X	US 5 097 833 A (CAMPOS JAMES M) 24 March 1992 (1992-03-24)	1,7,9		
A	* the whole document *	2-6,8,10		
Y	US 5 330 515 A (RUTECKI PAUL ET AL) 19 July 1994 (1994-07-19) * column 12, line 13-40; figures 1,4 *	8,10		
A	US 3 294 092 A (LANDAUER) 27 December 1966 (1966-12-27) * the whole document *	1-3,5,7-10		
A	US 5 397 338 A (GREY THOMAS L ET AL) 14 March 1995 (1995-03-14) * column 6, line 20-32 * * column 9, line 11-26; figure 5 *	1,2,5,7		TECHNICAL FIELDS SEARCHED (Int.Cl.7)
A	US 5 018 524 A (GU HANSEN ET AL) 28 May 1991 (1991-05-28) * column 2, line 31-68 * * column 4, line 44 - column 9, line 17; figures 1-8 *	1-4,7-10		A61N
The present search report has been drawn up for all claims				
Place of search THE HAGUE		Date of completion of the search 26 April 2001	Examiner Allen, E	
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EP 01 40 0186 (1999-03-18)

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 01 40 0186

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26-04-2001

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 4938223 A	03-07-1990	NONE	
US 5836081 A	17-11-1998	NONE	
US 5097833 A	24-03-1992	NONE	
US 5330515 A	19-07-1994	AU 4641493 A JP 8500988 T WO 9325271 A	04-01-1994 06-02-1996 23-12-1993
US 3294092 A	27-12-1966	NONE	
US 5397338 A	14-03-1995	EP 0642367 A WO 9422529 A	15-03-1995 13-10-1994
US 5018524 A	28-05-1991	CN 86102850 A AT 55548 T CA 1278045 A DE 3673478 D EP 0211159 A HK 31391 A JP 1705282 C JP 3070980 B JP 62106775 A SG 34391 G	04-11-1987 15-09-1990 18-12-1990 20-09-1990 25-02-1987 03-05-1991 27-10-1992 11-11-1991 18-05-1987 26-07-1991

EPC FORM P0439

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